•临床研究•

角度人工椎间盘置换后对相邻下位椎间隙 应力的影响

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【摘要】目的:探讨带角度人工颈椎间盘置换后椎间隙及相邻椎间隙应力变化。方法:根据已有的测量结果,设计角度人工椎间盘。对已建立的 $C_{4.5}$ 两节段带椎间盘的正常颈椎有限元模型、 $C_{4.5}$ 置换 0° 椎间盘假体和置换 10° 椎间盘假体后的颈椎模型进行轴向加压、前屈/后伸、侧弯、扭转加载,对比观察 $C_{4.5}$ 难间隙应力变化;对已建立的 C_4 — C_6 3 节段带椎间盘的正常颈椎有限元模型、 $C_{4.5}$ 置换 0° 椎间盘假体和置换 10° 椎间盘假体后的颈椎模型同样方式进行加载,对比置换节段及相邻节段的椎间隙应力变化。 结果: $C_{4.5}$ 两节模型加载中,轴向加载、前屈/后伸时 80 MPa/ 0° 假体与 80 MPa/ 10° 假体等效剪应力(Se)大小近似,较正常颈椎增大,侧弯时 80 MPa/ 0° 假体 Se 与正常颈椎接近,80 MPa/ 10° 假体 Se 较正常颈椎增大。扭转时加载时扭转切应力(Szx/Szy)80 MPa/ 0° 假体和 80 MPa/ 10° 假体接近正常颈椎。在 60 公司节段模型加载时,60 人。相同隙置换 60 MPa/60 化。相邻下位节段(60 的椎间隙 Se 均减小,扭转加载时 60 Szy/Szy 接近正常颈椎模型。 结论: 60 化间盘假体植入椎间隙对颈椎相邻节段的椎间隙应力影响小,接近正常颈椎间盘力学性能。

【关键词】 颈椎; 椎间盘; 生物力学 **DOI**: 10.3969/j.issn.1003-0034.2014.09.011

Effects of artificial disc replacement with angles on stress of adjacent intervertebral disc BAI Chuan-yi*, ZHANG Wei-jie, WEI Wen-bo, LING Wei, TIAN Zhen-xing, DANG Xiao-qian, and WANG Kun-zheng. * The First Department of Orthopaedics, the Second Affiliated Hospital of Medical College, Xi'an Jiaotong University, Xi'an 710004, Shaanxi, China

ABSTRACT Objective: To evaluate stress changes of intervertebral space and adjacent intervertebral space after artificial disc replacement with angles. **Methods**: Artificial disc replacement with angles were designed according to existing data. Axial pressure, flexion/extension, lateral bending and torsion loading were applied on finite element models of normal cervical discs on $C_{4,5}$ segments, $C_{4,5}$ segments with 0° artificial cervical discs and $C_{4,5}$ segments with 10° artificial cervical discs on C_{4} segments, $C_{4,5}$ segments with 0°, $C_{4,5}$ segments with 10°, then stress changes of replaced segments space and adjacent segment space were observed. **Results**: For $C_{4,5}$ segments, 80 MPa/0° artificial discs and 80 MPa/10° artificial discs had the similar equivalent shear stress(Se), and were both larger than that of normal discs, when lateral bending were performed, 80 MPa/10° artificial discs were closed to normal discs when axial pressure and flexion/extension were carried out, while 80 MPa/10° artificial discs had a larger Se than that of normal ones, when torsion loading were applied, Szx/Szy stress of 80 MPa/0° and 80 MPa/10° artificial discs were closed to normal ones. For C_4 – C_6 segments, the axial pressure, flexion/extension and lateral bending of $C_{5,6}$ were all lower than normal discs after $C_{4,5}$ discs were replaced by 80 MPa/10° artificial discs, while Szx/Szy of torsion loading were closed to normal ones. **Conclusion**: Artificial discs with 10° have less influences on stress of adjacent intervertebral space and closer to mechanical property after being implanted into intervertebral space.

KEYWORDS Cervical vertebrae; Intervertebral disk; Biomechnics

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研究表明[1-2]人工颈椎间盘置换术不能恢复手

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术节段的椎间角度,部分患者术后手术节段和生理曲度后凸,与终板后方打磨过度、假体植入角度、假体曲度结构缺失、后纵韧带的切除以及术前存在后凸有关,其中,假体曲度结构缺失是重要的因素。本研究根据西北地区人群颈椎间盘角度的基本数据^[3],设计了具有 10°的人工椎间盘假体,并利用精

细的颈椎有限元模型,对置换角度椎间盘后相邻下 位节段椎间隙的力学分析,评价角度椎间盘假体设 计的合理性。

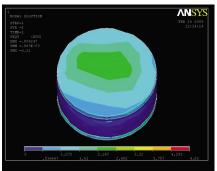
1 材料与方法

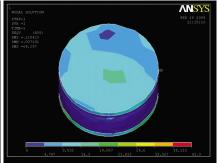
- 1.1 有限元模型建立主要设备、仪器和软件 ①GE-16 层螺旋 CT:GE 公司(美国)。②计算机:西安交通大学航天学院力学试验中心; 性能参数:CUP:Core i3 3220;内存:2 GB;硬盘:500 GB 串口;显存:1 GB;图形卡:Geforce;操作系统:Windows XP。 ③Mimics10.0 Materalise 公司(比利时)。④有限元软件 ANSYS11.0 ANSYS 公司(美国)。
- 1.2 试验方法 对已建立的包括椎间盘的 C_{4,5} 颈椎三维有限元模型进行力学加载^[4],获得正常颈椎加载后椎间盘的应力情况,摘除椎间盘并置换80 MPa/0°、80 MPa/10°假体后的颈椎模型加载,与正常模型的应力分析。同样对包括椎间盘的 C₄-C₆ 颈椎模型中 C_{4,5} 节段置换80 MPa/0°、80 MPa/10°假体后的颈椎模型加载,与正常模型加载后的应力对比分析。应力变化指标选择有限元计算常用的等效剪应力(Se)、Z轴方向的压应力(Sz)、扭转切应力(Szx/Szy)。分组:将有限元测试模型分为3组,分别为完整未手术组、置换80 MPa/0°假体组、置换80 MPa/10°假体组。
- 1.3 观察项目与方法 ①对颈椎带椎间盘 C_{4.5} 完整未手术、摘除 C_{4.5} 椎间盘置换弹性模量为 80 MPa 的 0°和 10°假体后的颈椎有限元模型分别进行轴向压缩、前屈/后伸、侧弯和扭转加载,轴向加载力50 N,前屈/后伸、侧弯和扭转运动加载力矩为

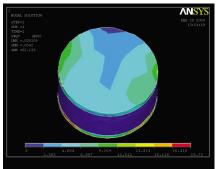
5 Nm,对比分析 C_{4,5} 椎间隙的应力及位移变化。②对 C₄-C₆ 3 节段颈椎完整未手术、摘除 C_{4,5} 椎间盘置换弹性模量为 80 MPa 的 0°和 10°假体后的颈椎有限元模型分别进行轴向压缩、前屈/后伸、侧弯和扭转加载,与正常模型对比分析 C_{4,5}、C_{5,6} 椎间隙的应力,观察置换假体节段的椎间隙及相邻节段椎间隙的应力变化。应力变化指标选择有限元计算常用的等效剪应力、Z 轴方向的压应力、扭转切应力。

2 结果

- **2.1** C_{4,5} 节段置换 80 MPa/0°、80 MPa/10°假体后椎间隙力学情况
- 2.1.1 应力分析 正常椎间盘与假体应力比较,轴向加载时人工椎间盘 Se 较正常颈椎增大明显,80 MPa/0°假体与80 MPa/10°假体应力大小近似;前屈/后伸时置换假体组 Se 较正常颈椎增大,80 MPa/0°假体与80 MPa/10°假体 Se 变化相同,角度改变对假体应力改变不明显。侧弯时80 MPa/0°假体 Se 与正常颈椎接近,80 MPa/10°假体 Se 较正常颈椎增大。扭转时 Szx/Szy 80 MPa/0°假体和80 MPa/10°假体接近正常颈椎。见表1,图 1-2。
- 2.1.2 位移分析 80 MPa/0°假体与80 MPa/10°假体置换后前屈/后伸、侧弯、扭转时位移与正常颈椎接近,0°与10°假体区别不明显,角度设计对椎间盘假体的位移影响不大。见表2。
- 2.2 C₄-C₆ 3 节颈椎模型及置换 80 MPa/10°假体后相邻(下位)椎间盘的应力分析 C_{4,5} 节段置换 80 MPa/10°假体后,置换节段的椎间隙应力在轴向加载、前屈/后伸、侧弯时,Se 减小不明显;扭转时







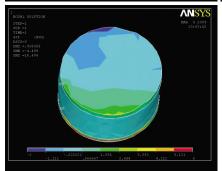


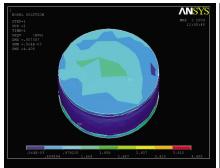
图 1 置换 80 MPa/0°假体 C_{4,5} 节段椎间隙应力云图(轴压、前屈、侧弯、扭转)

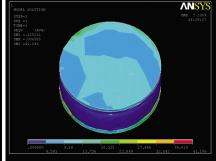
Fig.1 Stress map of $C_{4,5}$ intervertebral space when $C_{4,5}$ disc was replaced by 80 MPa/0° prosthesis (axial loading, flexion, lateral bending and rotation condition)

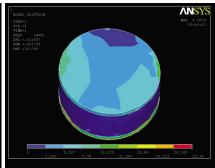
表 1 $C_{4,5}$ 节段置换 80 MPa/0°、80 MPa/10°假体置换后不同加载方式下力学情况(MPa)

Tab.1 Stress of vertebral disc when $C_{4,5}$ disc was replaced by 80 MPa/0°, 80 MPa/10° prosthesis under different loading models (MPa)

组别 -	轴向加载		前屈/后伸		侧弯		扭转	
	Se	Sz	Se	Sz	Se	Sz	Se	Szx/Szy
完整未手术组	1.0	1.3	10.7	9.4	4.5	6.4	3.6	1.65
置换 80 Mpa/0°假体组	2.4	0.4	14.0	13.6	4.4	6.5	12	1.56
置换 80 Mpa/10°假体组	2.6	0.3	14.0	4.7	8.0	0.7	8.7	1.4







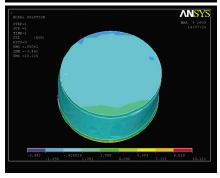


图 2 置换 80 MPa/10°假体 C_{4.5} 节段椎间隙应力云图(轴压、前屈、侧弯、扭转)

Fig.2 Stress map of $C_{4,5}$ intervertebral space when $C_{4,5}$ disc was replaced by 80 MPa/10° prosthesis (axial loading, flexion, lateral bending and rotation condition)

表 2 C_{4,5} 节段置换 80 MPa/0°、80 MPa/10°假体置换后 不同加载方式下位移情况(mm)

Tab.2 Displacement when $C_{4,5}$ disc was replaced by 80 MPa/ 0° , 80 MPa/ 10° prosthesis under different loading models (mm)

组别	前屈/后伸	侧弯	扭转
完整未手术组	0.08	0.01	0.03
置换 80 MPa/0°假体组	0.11	0.02	0.28
置换 80 MPa/10°假体组	0.11	0.02	0.23

Szx/Szy 改变不明显,接近正常状态。相邻下位节段 (C_{5,6})的 Se 在轴向加载、前屈/后伸、侧弯时减小,接 近正常模型状态,扭转时与正常颈椎相同。见表 3, 图 3-4。

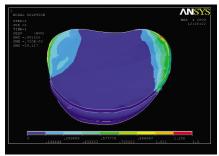
3 讨论

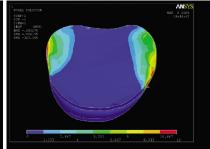
3.1 椎间盘的生物力学及融合固定后应力改变研究表明,椎间盘在压缩应力下负荷最大,压缩前屈时应力增加到原 113%,压缩后伸时 14%,侧弯时68%,旋转时 75%。退变的椎间盘受到外力时载荷分

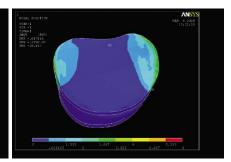
表 3 $C_{4,5}$ 节段置换 80 MPa/10°假体后不同加载方式下椎间盘应力改变(MPa)

Tab.3 Stress of vertebral disc when C_{4,5} disc was replaced by 80 MPa/10° prosthesis under different loading models(MPa)

组别	椎间隙 —	轴向加载		前屈/后伸		侧弯		扭转	
		Se	Sz	Se	Sz	Se	Sz	Se	Szx/Szy
完整未手术组	C _{4,5}	2.80	1.50	15.80	4.60	15.00	7.50	0.16	0.01
	$C_{5,6}$	0.43	0.74	5.60	7.90	2.00	2.30	2.80	1.00
置换 80 MPa/0°假体组	$C_{4,5}$	1.30	0.28	13.10	6.30	5.92	3.89	6.63	0.88
	$C_{5,6}$	0.21	0.42	4.10	4.73	1.12	1.98	2.23	0.96
置换 80 MPa/10°假体组	$C_{4,5}$	1.50	0.32	13.80	6.60	6.70	4.50	7.00	0.90
	$C_{5,6}$	0.30	0.54	4.60	4.80	1.33	2.10	3.10	1.00







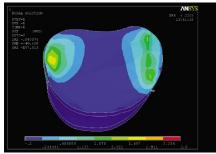
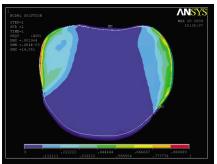
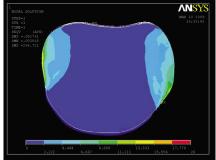
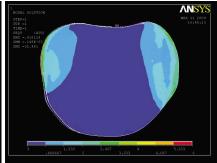


图 3 正常 3 节段颈椎 C₄-C₆ 加载后 C_{5,6} 节段椎间隙应力云图 (轴压、前屈、侧弯、扭转)

 $\label{eq:Fig.3} \textbf{Fig.3} \quad \text{Stress map of $C_{5,6}$ intervertebral space when intacting on C_4-C_6 model (axial loading, flexion, lateral bending and rotation condition)}$







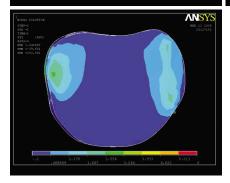


图 4 C_{4,5} 节段置换 80 MPa/10°假体后相邻 C_{5,6} 节段椎间隙应力云图(轴压、前屈、侧弯、扭转)

Fig.4 Stress map of $C_{5,6}$ facet joints when $C_{4,5}$ disc was replaced by 80 MPa/10° prosthesis (axial loading, flexion, lateral bending and rotation condition)

布发生改变,引起椎间盘损伤的主要载荷是弯曲载荷和扭转载荷^[5]。正常椎间盘具有良好的黏弹性,因此颈椎有很好的屈曲蠕变能力和应力松弛性能,以适应人体正常活动,在过度屈曲或后伸状态下,应力水平很难维持^[6]。黏弹特性使椎间盘能有效缓冲和传递负荷,颈椎间盘假体的设计应使假体的弹性模量接近正常椎间盘,以达到最佳的仿生效果和接近生理状态力学性能。前方椎间盘和后方双侧关节突关节构成了运动节段的稳定,称关节三联体结构,三者中任一结构退变将引起整个椎间关节力学改变。颈椎椎间盘退变时,髓核水份减少,椎间高度降低,分布在关节突关节的压力明显增大,关节突之间运

动会造成关节突慢性损伤,并导致关节突肥大、增生,继而引发临床症状[7]。

颈前路减压植骨融合内固定术,植入的骼骨和金属内固定的刚度都比椎间盘的大,易产生应力遮挡,椎间融合后可活动的椎间节段减少,为了维持颈椎整体的活动度,相邻节段椎间的活动度将增加,过渡的活动将加速邻近节段的退变^[8],甚至包含融合节段上下超过一个间隙范围的未融合运动节段的退行性病变。Clavenna等^[9]通过对尸体标本进行颈椎融合模拟手术后行生物力学测试,发现融合节段活动度减少达到 66.5%,融合节段上下节段的活动度均增加。Kelly等^[10]对行单节段颈椎融合术后的患者

进行了随访,结果显示融合上节段活动度较术前增加了1.4°,融合下节段活动度较术前增加了2.6°。

3.2 人工椎间盘置换对椎间隙应力影响 Koller 等[11]对 19 例行 Discover 颈椎间盘假体置换的患者 进行了15个月的随访,发现手术节段的活动度与术 前无明显差异,相邻节段未出现明显的应力增加。研 究表明:Bryan 人工颈椎间盘置换后下位节段椎间隙 的压力变化在前屈、后伸、侧弯、扭转下与椎间盘完 整状态均无明显差异,提示 Bryan 人工颈椎间盘可 以达到颈椎生物力学性能重建的要求。Ren 等[12]对 Bryan 人工颈椎间盘置换术后的患者进行 2~6 年随 访,相邻椎间隙的应力未发生明显改变,置换节段的 活动度可长期保留。Garrido 等[13]将 47 例颈椎病患 者随机分为 Bryan 人工颈椎间盘置换组和颈前路减 压植骨融合术(ACDF)组分别进行治疗,术后平均随 访时间为48个月,结果显示置换组相邻节段活动度 较术前未见明显差异。本试验中80 MPa/0°假体置 换后,同节段椎间隙轴向加载、前屈/后伸时椎间盘 Se 应力增大明显,说明假体的整体弹性模量偏大使 假体本身应力水平提高,应力集中在假体。侧弯和扭 转时应力和正常椎间隙应力接近,较接近生理状态。

3.3 置换 80 MPa/10°假体对相邻椎间隙应力影响颈椎的生理前凸,可以吸收振荡、减轻重力缓冲。颈椎前后力量改变时,颈椎曲度改变是适应新的力失衡的结果,颈椎曲度改变后导致周围的血管和神经张力改变,继而产生症状。Stemper等[14]研究发现,颈椎的曲度改变后可出现轴性症状,如颈痛、颈部僵硬、肢体麻木、肩痛、肩胛间痛等,说明颈部轴性症状与颈椎曲度改变密切相关。Kawakami等[15]研究发现,约50%的患者减压植骨内固定术后出现了轴位综合征,查找原因并对比患者情况,两组中惟一有统计学差异的因素就是生理前凸的正常与否。许多学者发现颈椎术后轴性症状与颈椎前凸弧度大小密切相关,颈椎轴性症状重的患者颈椎前凸小[10,16]。

颈椎后凸畸形是 Bryan 椎间盘假体置换术后较常见的并发症,术后手术节段发生后凸的患者约15.6%,全颈椎发生后凸约14.3%,原因除了和手术操作有关,假体曲度结构缺失也是重要的因素[17-18]。角度椎间盘假体的设计维持手术节段的椎间隙角度,或可改善颈椎生理曲度。

本试验中,C_{4.5} 节段置换 80 MPa/10°椎间盘假体后,同节段椎间隙在轴向加载、前屈/后伸椎间隙应力增大明显,侧弯时扭转时 Se 增大,原因是假体角度的加大使加载力向后分解,关节突关节有滑移特性,模型未加约束,减缓了应力,扭转时 Szx/Szy 应力时与正常颈椎模型加载接近。在 C₄-C₆ 3 节段模型

加载时, C_{4,5} 节段置换 80 MPa/10°假体后,轴向加载、前屈/后伸、扭转加载时,相邻下位节段(C_{5,6})的椎间隙应力在轴向加载、前屈/后伸、侧弯时均减小,扭转时 Szx/Szy 接近正常颈椎模型力学特性,说明80 MPa/10°椎间盘假体植入椎间隙对颈椎相邻节段的椎间隙应力影响小,能够起到正常椎间盘的作用并维持椎间角度。

假体在外力下的形变与假体本身刚度相关,而各同质材料的刚度取决于其弹性模量和剪切模量。各公司设计的假体角度不同,是根据假体材料的弹性模量不同而设计的。本研究对假体材料弹性模量为80 MPa 情况下对10°和0°假体作力学比较,观察角度的改变对颈椎力学的影响。进一步研究中将增加人尸体标本生物力学试验与三维有限元模型对照,验证有限元研究的准确性。进行动物实验体内植入观察假体的长期力学性能,观察角度椎间盘假体置换能否恢复手术节段的椎间盘角及颈椎生理曲度,为进一步在临床应用提供实验依据。

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《中国骨伤》杂志 2015 年重点专题征稿通知

《中国骨伤》杂志本着坚持中西医并重原则,突出中西医结合特色的办刊宗旨,如期发布 2015 年征稿通知。以下是《中国骨伤》杂志 2015 年重点专题征稿的范围,欢迎广大的读者和作者踊跃投稿。

- 1. 颈腰椎疾病微创治疗方法 (现代技术与传统方法的开发应用)的选择
- 2. 腰椎间盘局限性高信号区(HIZ)与椎间盘内紊乱(IDD) 的相关性
- 3. 脊髓损伤的早中期的诊疗及规范
- 4. 人工关节置换术围手术期的相关问题
- 5. 老年关节置换围手术期处理和术前风险评估
- 6. 骨关节炎选择关节镜手术时的误区
- 7. 人工关节翻修术常见疑难问题的处理

- 8. 踝关节骨折畸形愈合的手术治疗
- 9. 关节镜在肩、肘、足踝和髋关节等疾病中应用
- 10. 髋臼骨折术后并发症的处理
- 11. 肢体畸形的修复与重建
- 12. 四肢开放性骨折伴软组织缺损的处理
- 13. 骨与软组织肿瘤的诊断、治疗和预后
- 14. 股骨头坏死外科分期治疗和远期疗效评价
- 15. 手法治疗在脊柱、关节和创伤疾病中的应用和探讨
- 16. 中医微创手术在脊柱、关节、创伤疾病中的应用和探讨

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